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71 **ABSTRACT**

72 **Background:** Right ventricular (RV) function is an important predictor of morbidity and  
73 mortality in various cardiovascular conditions. Nevertheless, its echocardiographic assessment is  
74 challenging due to its complex anatomy and location in the chest, resulting in limited inter-  
75 observer reproducibility.

76 **Objectives:** We aimed to develop a novel deep learning model – **EchoNet-RV** – to segment the  
77 RV in apical 4-chamber view (A4C) echocardiographic videos and estimate RV fractional area  
78 change (RVFAC).

79 **Methods:** For training EchoNet-RV, 7,169 expert-annotated A4C echocardiographic videos  
80 were used. The model’s performance was evaluated on a held-out internal test set of 1,320 A4C  
81 videos and two international external test sets of 3,107 and 1,077 A4C videos from two separate  
82 centers. Additionally, the associations between the predicted RVFAC values and the composite  
83 endpoint of heart failure hospitalization or all-cause death were also analyzed in the first external  
84 test set.

85 **Results:** EchoNet-RV segmented the RV with Dice coefficients of 0.893 (0.891–0.895), 0.797  
86 (0.796–0.798), and 0.788 (0.785–0.790) and predicted RVFAC with mean absolute errors of  
87 5.795 (5.560–6.031), 5.830 (5.692–5.970), and 6.362 (6.064–6.660) percentage points in the  
88 held-out test set and the two external test sets, respectively. In 500 randomly selected videos  
89 from the external test sets, EchoNet-RV’s prediction error was significantly lower than the inter-  
90 observer variability ( $p < 0.001$ ). Moreover, it identified RVFAC  $< 35\%$  with areas under the  
91 receiver operating characteristic curve of 0.859 (0.843–0.876), 0.725 (0.710–0.740), and 0.684  
92 (0.653–0.713) in the three test sets. EchoNet-RV also outperformed two multi-task models,  
93 EchoPrime and PanEcho, in estimating RVFAC and identifying RV dysfunction in the external

94 test sets. In the first external test set, predicted RVFAC values were inversely associated with the  
95 composite endpoint (adjusted HR: 0.948 [0.917–0.979],  $p < 0.001$ ), independent of age, sex,  
96 cardiovascular risk factors, and left ventricular systolic function.

97 **Conclusions:** EchoNet-RV enables the rapid and automated assessment of RVFAC, with strong  
98 potential to become a valuable tool for the echocardiographic evaluation of RV function and  
99 disease surveillance.

100

101 **Keywords:** right ventricle; right ventricular fractional area change; echocardiography; artificial  
102 intelligence; deep learning

103 **CONDENSED ABSTRACT**

104           In this study, we developed EchoNet-RV, an echocardiography-based DL model for  
105 automated RV segmentation and RVFAC estimation, and evaluated its performance on two  
106 international external datasets. EchoNet-RV demonstrated robust performance in RV  
107 segmentation, RVFAC estimation, and RV dysfunction detection, with prediction errors  
108 significantly lower than inter-observer variability. It also outperformed two multi-task models,  
109 EchoPrime and PanEcho, in estimating RVFAC and identifying RV dysfunction. Moreover, the  
110 model’s predictions were also associated with adverse clinical outcomes. EchoNet-RV enables  
111 rapid and automated RVFAC assessment, with strong potential to become a valuable tool for the  
112 echocardiographic evaluation of RV function and disease surveillance.

113 **ABBREVIATIONS**

114

115 A4C = apica 4-chamber view

116 AI = artificial intelligence

117 AUC = area under the receiver operating characteristic curve

118 CNN = convolucional neural network

119 CV = coefficient of variation

120 DL = deep learning

121 ICC = intraclass correlation coefficient

122 LOA = limit of agreements

123 MAD = mean absolute difference

124 MAE = mean absolute error

125 MDC = minimal detectable change

126 MMH = MacKay Memorial Hospital

127 RVFAC = right ventricular fractional area change

128 TAPSE = tricuspid annular plane systolic excursion

129 S' = tricuspid annular peak systolic velocity by tissue Doppler imaging

130 SEM = standard error of measurement

131 **INTRODUCTION**

132 Right ventricular (RV) function is a key determinant of quality of life, exercise capacity,  
133 morbidity, and mortality across a wide range of cardiopulmonary diseases (1,2). Therefore,  
134 accurate detection and continuous surveillance of RV dysfunction are pivotal in routine clinical  
135 practice. To date, echocardiography remains the first-line imaging modality for assessing RV  
136 structure and function (1). However, large national and international echocardiography surveys  
137 have consistently reported that the majority of clinicians assess RV function only qualitatively  
138 (3-5). This reliance on qualitative evaluation reflects the inherent challenges of evaluating the  
139 complex anatomy and contraction pattern of the RV using two-dimensional echocardiography  
140 (6), as well as the persistent issues with standardization in image acquisition, analysis, and  
141 reporting (7). These limitations contribute to the underutilization of RV functional parameters in  
142 clinical decision-making and their limited incorporation into clinical guidelines (7).

143 Unlike tricuspid annular plane systolic excursion (TAPSE) and tricuspid annular peak  
144 systolic velocity by tissue Doppler imaging (S') (i.e., the most widely used quantitative metrics),  
145 RV fractional area change (RVFAC) not only the longitudinal shortening of the RV but also its  
146 radial contractions and the contribution of the interventricular septum, resulting in a strong  
147 correlation with cardiac magnetic resonance imaging-derived RV ejection fraction (8).  
148 Accordingly, the 2025 American Society of Echocardiography guidelines for right heart  
149 assessment recommend RVFAC to be incorporated as a standard component into the  
150 echocardiographic evaluation of RV function (9). However, even in well-controlled research  
151 settings, RVFAC measurements show considerable heterogeneity and inter-observer variability  
152 (10-12). This variability arises from reliance on reader experience, inconsistencies in image

153 quality, and persistent standardization challenges related to RVFAC measurement, as outlined  
154 above.

155         With the growing adoption of artificial intelligence (AI)-based semantic segmentation  
156 models in cardiovascular imaging (13-15), these technologies may offer a promising solution to  
157 current challenges by improving measurement consistency and enhancing generalizability, while  
158 also expanding access to automated RV function quantification. AI-based measurements have  
159 been shown to reduce intra-observer variability in a blinded comparison with echocardiographer  
160 assessments (16), and numerous deep learning (DL) models have been developed to automate  
161 labor-intensive manual tasks such as contouring and annotation of echocardiographic images  
162 (17-19). Beyond automation, AI-augmented qualitative and quantitative assessment of cardiac  
163 structure and function may also reveal subclinical changes in cardiac physiology (20,21).

164         Accordingly, we aimed to develop a novel DL model – EchoNet-RV – to segment the RV  
165 in apical 4-chamber view (A4C) echocardiographic videos and predict RVFAC (Central  
166 Illustration). We hypothesized that this model would provide reliable and reproducible RVFAC  
167 measurements in a fully automated manner, facilitating scalable and objective RV function  
168 assessment. Beyond extensively evaluating EchoNet-RV’s performance in three geographically  
169 distinct cohorts, we also aimed to analyze the associations between the predicted RVFAC values  
170 and clinical outcomes to prove the prognostic capabilities of the model.

171 **METHODS**

172 **Datasets**

173 *Stanford dataset*

174           The Stanford dataset, used for model development and internal validation, comprised a  
175 total of 8,489 A4C videos from 8,314 studies of 5,386 patients who underwent transthoracic  
176 echocardiography between 2016 and 2018 as part of clinical care at Stanford Health Care  
177 (California, USA). Videos were acquired using Philips iE33, Philips EPIQ 5G, Philips EPIQ 7C,  
178 or Siemens Acuson SC2000 ultrasound machines. In this dataset, each video represents a unique  
179 study. Videos were randomly split into three sets of 5,892, 1,277, and 1,320 videos for training,  
180 validation, and testing, respectively. Splitting was performed at the patient level to avoid  
181 including videos from the same patient in more than one of the three sets. Clinical characteristics  
182 of the entire Stanford dataset and its three subsets are summarized in Supplemental Table 1,  
183 whereas technical details of the videos are presented in Supplemental Table 2.

184

185 *Semmelweis dataset*

186           The Semmelweis dataset, used for external validation and for assessing the prognostic  
187 value of the predicted RVFAC values, consisted of a total of 3,107 A4C videos from 982 studies  
188 of 872 patients who underwent transthoracic echocardiography between 2013 and 2021 at the  
189 Heart and Vascular of Semmelweis University (Budapest, Hungary). Clinical characteristics of  
190 these patients are summarized in Table 1, whereas technical details of the videos are presented in  
191 Supplemental Table 3. For patients included in the present study, mortality data were obtained  
192 from Hungary's National Health Insurance Database, whereas information on heart failure  
193 hospitalizations was collected through chart review.

194

195 *MacKay Memorial Hospital dataset*

196         The MacKay Memorial Hospital (MMH) dataset, also used for external validation,  
197 included a total of 1,077 A4C videos from 1,077 studies of 1,077 patients who underwent  
198 transthoracic echocardiography between 2009 and 2022 at MacKay Memorial Hospital (Taipei,  
199 Taiwan). Clinical characteristics of these patients are summarized in Table 1, whereas technical  
200 information regarding the videos is provided in Supplemental Table 3.

201

202 **Video annotation**

203         For each video in all three datasets, the endocardial border of the RV was manually  
204 traced by experienced echocardiographers in end-diastolic and end-systolic frames to assess the  
205 corresponding RV areas, which were then used to calculate RVFAC. In the Stanford dataset,  
206 manual contouring was performed in only one end-diastolic and one end-systolic frame per  
207 video, whereas in the two external test sets, contouring was performed in up to three cardiac  
208 cycles, when feasible. If contouring was performed in multiple cardiac cycles, RVFAC values  
209 were calculated using end-diastolic and end-systolic area pairs from each cardiac cycle and  
210 averaged to derive a single RVFAC label for the video. Of note, EchoNet-RV was trained using  
211 both the human expert-drawn RV contours (i.e., segmentation masks) of the sparsely annotated  
212 frames and the video-level RVFAC values. In addition, an experienced echocardiographer  
213 reviewed all videos of both external test sets to assess image quality using a 5-point Likert scale  
214 (nondiagnostic, poor, moderate, good, excellent) and to determine the view type (standard or  
215 RV-focused A4C), thereby enabling the analysis of these factors' impact on model performance.

216

## 217 **Video preprocessing**

218 An automated preprocessing pipeline was used to remove identifying information and  
219 burnt-in annotations, and to convert videos exported as DICOM files into a standardized format  
220 suitable for DL analysis. First, each video was square-cropped and masked to eliminate text and  
221 any other information outside the scanning sector. The resulting square frames were  
222 subsequently down-sampled to standardized 112×112-pixel videos using cubic interpolation and  
223 saved as AVI files.

224

## 225 **Architecture and development of EchoNet-RV**

226 EchoNet-RV comprises two key modules, similar to EchoNet-Dynamic (13). The first  
227 module is a convolutional neural network (CNN) that uses a DeepLabV3 (22) architecture with a  
228 ResNet-50 backbone to perform frame-level semantic segmentation of the RV. Even though the  
229 data used for training this module was only sparsely annotated (i.e., human annotations were  
230 available for only some of the end-diastolic and end-systolic frames), the chosen architecture was  
231 well-suited for this form of weakly supervised learning, and generalized well throughout the  
232 cardiac cycle, even to frames that did not contain annotations (Figure 1A). The model was  
233 trained for 50 epochs using pixel-wise cross-entropy loss and a stochastic gradient descent  
234 optimizer with a learning rate of 1e-5, a momentum of 0.9, and a batch size of 20. The weights  
235 from the epoch with the lowest validation loss were selected for final testing.

236 The second module is a spatiotemporal CNN with an R(2+1)D-18 (23) architecture that  
237 directly estimates RVFAC from each video without relying on segmenting the RV. During the  
238 training of this module, 16 frames were sampled by taking every other frame from the video as  
239 input. To simulate slight translations and changes in transducer position, training videos were

240 padded by 12 pixels on each side, followed by a random crop of the original frame size. The  
241 model was trained for 45 epochs using a stochastic gradient descent optimizer with a learning  
242 rate of  $1e-4$ , a momentum of 0.9, and a batch size of 20.

243         Given that substantial beat-to-beat variation in the end-diastolic and end-systolic RV  
244 areas (and thus in RVFAC) can occur in several cardiac conditions, such as atrial fibrillation and  
245 premature atrial or ventricular contractions, test-time augmentation was also applied to obtain  
246 robust final predictions. Experiments were conducted using two different approaches (Figure 2).  
247 The first approach followed the method used in EchoNet-Dynamic (13). Briefly, each ventricular  
248 contraction (i.e., the systolic phase of the cardiac cycle) was identified by selecting the frames  
249 between the largest and smallest RV areas predicted by the segmentation model. For each  
250 identified contraction (i.e., beat), 32-frame video clips centred around the ventricular contraction  
251 were obtained and processed by the spatiotemporal CNN module to produce beat-to-beat  
252 estimates of RVFAC, which were then averaged to yield the final video-level output of EchoNet-  
253 RV. In contrast, the second approach did not rely on the segmentation model’s output. Instead, it  
254 randomly sampled 5 (possibly overlapping) 32-frame video clips from each video, and individual  
255 predictions generated by the spatiotemporal CNN module from these 5 clips were averaged to  
256 produce the final video-level model output. The approach achieving superior performance in the  
257 held-out test set was adopted as the ultimate test-time augmentation technique in the final  
258 EchoNet-RV model, and the results are reported accordingly.

259         Preprocessing and model development were performed in Python (version 3.15) using the  
260 PyTorch DL library (version 1.8.0). Models were trained on a server equipped with four  
261 NVIDIA GeForce RTX 2080 Ti graphics processing units. To facilitate further research and

262 potential deployment, the public repository containing the source code and model weights of  
263 EchoNet-RV is available at <https://github.com/echonet/RV>.

264

### 265 **Comparing prediction error with beat-to-beat and inter-observer variability**

266 To compare EchoNet-RV’s prediction error with beat-to-beat variability, videos of the  
267 external test sets with human measurements of RVFAC in 2 or more cardiac cycles (n=3,943)  
268 were used. To compare the model’s prediction error with inter-observer variability, 250 videos  
269 from each of the Semmelweis and MMH datasets were randomly sampled, and RVFAC was  
270 remeasured by a second reader blinded to the first reader’s measurements. These repeated  
271 measurements were used for quantifying prediction error, beat-to-beat variability, and inter-  
272 observer variability. Metrics and statistical tests used in the analyses are described in the  
273 subsection on performance metrics.

274

### 275 **Benchmarking against multi-task models**

276 EchoNet-RV’s performance was also compared with two recently published multi-task  
277 DL models for comprehensive echocardiogram interpretation – EchoPrime (21) and PanEcho  
278 (20) – in the external test sets. While EchoPrime estimates RVFAC as a continuous variable,  
279 PanEcho can only classify RV systolic function as normal or reduced. Therefore, the  
280 performance of EchoNet-RV and EchoPrime could be compared both in estimating RVFAC and  
281 in detecting RV dysfunction, whereas benchmarking against PanEcho was possible only for the  
282 latter task.

283

284 **Analyzing associations with outcomes**

285 Associations between the predicted RVFAC values and outcomes were analyzed in the  
286 Semmelweis dataset. In the present study, the outcomes of interest were the composite endpoint  
287 of heart failure hospitalization or all-cause death, as well as all-cause death alone.

288

289 **Performance metrics and statistical analysis**

290 EchoNet-RV's performance in the semantic segmentation task was evaluated using the  
291 Dice similarity coefficient, whereas its performance in the RVFAC estimation task was assessed  
292 using the mean absolute error (MAE) and the intra-class correlation coefficient (ICC). Absolute  
293 errors between subgroups were compared using the unpaired Student's t-test or the Mann-  
294 Whitney U test, as appropriate. The trend between image quality categories and absolute errors  
295 was assessed using the Jonckheere-Terpstra test. Bland-Altman analysis was performed to  
296 calculate the bias and limits of agreement (LOA). Additionally, an extended version of the  
297 Bland-Altman analysis, incorporating inverse weighting, defining a clinically relevant range of  
298 interest, and quantifying the trend between means and differences, was also performed, as  
299 proposed by Padeloup et al. (24). In the present study, the range of interest for RVFAC was 15–  
300 45%, corresponding to the clinically relevant spectrum observed across the datasets. The model's  
301 performance in detecting RV dysfunction (defined as RVFAC <35%) was quantified using the  
302 area under the receiver operating characteristic curve (AUC), and accuracy, specificity,  
303 sensitivity, negative predictive value, and positive predictive value were also computed after  
304 dichotomizing the predicted and human-measured RVFAC values using the guideline-  
305 recommended cutoff value of 35% (9). To evaluate EchoNet-RV's prediction error in the context  
306 of beat-to-beat and inter-observer variability, mean absolute difference (MAD), standard error of

307 measurement (SEM), minimal detectable change (MDC), and coefficient of variation (CV) were  
308 computed in subsets of videos. MADs were compared using paired Student's t-tests or Wilcoxon  
309 signed-rank tests, whereas the significance of the difference in SEM, MDC, and CV was  
310 determined using bootstrap p-values. When benchmarking the performance of EchoNet-RV  
311 against other models, absolute errors were compared using paired Student's t-tests or Wilcoxon  
312 signed-rank tests, whereas AUCs were compared using the DeLong test. For each of the  
313 aforementioned performance metrics, 95% confidence intervals (CIs) were calculated from  
314 10,000 stratified bootstrap resamples. Results are reported at the video level unless stated  
315 otherwise.

316 Continuous variables are expressed as median (interquartile range), while categorical  
317 variables are reported as frequencies and percentages. The event-free survival of subgroups was  
318 visualized on Kaplan-Meier curves, and Log-rank tests were performed for comparison. In  
319 patients with follow-up longer than 5 years and no events during that period, right censoring was  
320 applied at 5 years. Cox proportional hazards models were used to compute hazard ratios with  
321 95% CIs. All survival analyses were performed at the patient level. A p-value of <0.05 was  
322 considered statistically significant.

323

## 324 **Ethical approval**

325 The study protocol conforms with the principles outlined in the Declaration of Helsinki,  
326 and it was approved by the Institutional Review Boards of Stanford University and Cedars-Sinai  
327 Medical Center, the Regional and Institutional Committee of Science and Research Ethics of  
328 Semmelweis University (approval number: 190/2020), and the Institutional Review Board of  
329 MacKay Memorial Hospital (study identifier: 25MMHIS019e). Obtaining informed consent was

330 waived due to the retrospective nature of the analysis. Methods and results are reported in  
331 compliance with the updated Proposed Requirements for Cardiovascular Imaging-Related  
332 Multimodal-AI Evaluation (PRIME 2.0) checklist (Supplemental Table 4) (25).

## 333 **RESULTS**

### 334 **Performance in RV segmentation**

335 EchoNet-RV segmented the RV in all human-annotated end-diastolic and end-systolic  
336 frames with Dice coefficients of 0.893 (95% CI: 0.891–0.895), 0.797 (95% CI: 0.795–0.798),  
337 and 0.788 (95% CI: 0.785–0.790) in the held-out internal test set and Semmelweis and MMH  
338 datasets, respectively (Figure 1B–C). When considering only end-diastolic frames, it achieved  
339 Dice coefficients of 0.903 (95% CI: 0.900–0.905), 0.815 (95% CI: 0.813–0.816), and 0.807  
340 (95% CI: 0.805–0.810) in these three datasets, whereas in end-systolic frames only, the Dice  
341 coefficients were 0.883 (95% CI: 0.880–0.886), 0.779 (95% CI: 0.777–0.781), and 0.768 (95%  
342 CI: 0.764–0.772), respectively (Figure 1B–C).

343

### 344 **Performance in RVFAC prediction**

345 Among the two evaluated test-time augmentation strategies, random sampling of 5 clips  
346 yielded a slightly lower MAE than beat-to-beat sampling (5.795 [95% CI: 5.520–6.070] vs.  
347 5.833 [95% CI: 5.555–6.113] percentage points) in the held-out test set; therefore, this approach  
348 was adopted in the final EchoNet-RV model.

349 EchoNet-RV predicted RVFAC with MAEs of 5.795 (95% CI: 5.560–6.031), 5.830 (95%  
350 CI: 5.692–5.970), and 6.362 (95% CI: 6.064–6.660) percentage points and ICCs of 0.648 (95%  
351 CI: 0.616–0.677), 0.481 (95% CI: 0.452–0.509), and 0.301 (95% CI: 0.243–0.356) in the held-  
352 out test set and the Semmelweis and MMH datasets, respectively (Figure 3A). Conventional  
353 Bland-Altman analysis showed biases of 0.233, 1.275, and -2.635 percentage points, along with  
354 LOA widths of 30.260, 28.837, and 29.987 percentage points, in the three test sets (Figure 3B).  
355 Extended Bland-Altman analysis, which is less affected by the distribution differences between

356 datasets (24,26), showed biases of 0.433, 1.875, and -0.228 percentage points, LOA widths of  
357 29.765, 31.221, and 29.651 percentage points, and slopes of the mean-difference relationship of -  
358 0.318, -0.210, and -0.354, respectively (Figure 3C). Given that multiple A4C videos were  
359 extracted from the same echocardiographic study in the Semmelweis dataset, study-level MAE  
360 and ICC were also calculated, yielding 4.744 (95% CI: 4.541–4.943) percentage points and 0.573  
361 (95% CI: 0.526–0.617), respectively.

362 Although EchoNet-RV's prediction error was higher than the beat-to-beat variability of a  
363 reader's measurements within the same video (all  $p < 0.001$ , Table 2), it was lower than the inter-  
364 observer variability (all  $p < 0.001$ , Table 3).

365 In the external test sets, subgroup analyses were also performed to analyze the differences  
366 in performance between videos acquired using different ultrasound machines and the impact of  
367 view type and image quality on prediction performance (Figure 4, Supplemental Table 5). These  
368 analyses revealed that the EchoNet-RV performed slightly better on videos acquired using GE  
369 ultrasound machines than those acquired using Philips (Semmelweis dataset:  $p < 0.001$ ; MMH  
370 dataset:  $p = 0.031$ ). Errors were similar in standard and RV-focused A4C videos in both external  
371 test sets (Semmelweis dataset:  $p = 0.406$ ; MMH dataset:  $p = 0.072$ ), whereas they showed a  
372 decreasing trend with better image quality in the Semmelweis dataset ( $p < 0.001$ ), but not in the  
373 MMH dataset ( $p = 0.373$ ).

374

### 375 **Performance in identifying RV dysfunction**

376 RV dysfunction (defined as RVFAC  $< 35\%$ ) was present in 878 (66.5%), 1,732 (55.7%),  
377 and 275 (25.5%) videos in the held-out test set and the Semmelweis and MMH datasets,  
378 respectively. EchoNet-RV identified RV dysfunction with AUCs of 0.859 (95% CI: 0.843–

379 0.876), 0.725 (95% CI: 0.710–0.740), and 0.684 (95% CI: 0.653–0.713) in these three test sets,  
380 respectively (Figure 5). In the Semmelweis dataset, study-level AUC was 0.770 (95% CI: 0.746–  
381 0.794). Other performance metrics for this task are reported in Supplemental Table 6.

382

### 383 **Benchmarking against multi-task models**

384 EchoNet-RV predicted RVFAC with lower absolute errors than EchoPrime in both the  
385 Semmelweis (5.830 [95% CI: 5.670–5.992] vs. 6.171 [95% CI: 6.002–6.339],  $p=0.001$ ) and  
386 MMH datasets (6.362 [95% CI: 6.064–6.660] vs. 6.728 [95% CI: 6.406–7.048],  $p=0.009$ ) (Table  
387 4). Moreover, EchoNet-RV achieved higher AUCs for identifying RV dysfunction than both  
388 EchoPrime and PanEcho in the Semmelweis dataset (0.727 [95% CI: 0.709–0.744] vs. 0.683  
389 [95% CI: 0.664–0.701] and vs. 0.673 [95% CI: 0.654–0.692], both  $p<0.001$ ), whereas  
390 comparable AUCs were observed in the MMH dataset (0.684 [95% CI: 0.648–0.719] vs. 0.652  
391 [95% CI: 0.614–0.690] and vs. 0.657 [95% CI: 0.619–0.695],  $p=0.220$  and  $p=0.150$ ,  
392 respectively) (Table 4).

393

### 394 **Associations with outcomes**

395 In the Semmelweis dataset, 125 (14.3%) patients reached the composite endpoint of heart  
396 failure hospitalization or all-cause death, whereas 110 (12.6%) died during the follow-up  
397 duration of 5.0 (4.2–5.0) years. Univariable Cox regression analyses showed that the higher  
398 values of EchoNet-RV-predicted RVFAC were associated with a lower risk of the composite  
399 endpoint (undadjusted HR: 0.877 [95% CI: 0.855–0.900],  $p<0.001$ ) and all-cause death  
400 (undadjusted HR: 0.877 [95% CI: 0.854–0.901],  $p<0.001$ ) (Tables 5 and 6). Moreover, predicted  
401 RVFAC was also an independent predictor of these adverse outcomes in multivariable Cox

402 regression models (composite endpoint – adjusted HR: 0.943 [95% CI: 0.912–0.975],  $p < 0.001$ ;  
403 all-cause death – adjusted HR: 0.932 [95% CI: 0.899–0.965],  $p < 0.001$ ) that included age, sex,  
404 coronary artery disease, heart failure, hypertension, diabetes, chronic kidney disease, and left  
405 ventricular ejection fraction as covariates (Tables 5 and 6). The prognostic value of the model's  
406 predictions was also confirmed by Kaplan-Meier curves of subgroups created based on the  
407 guideline-recommended RVFAC cutoff value of 35% (Figure 6).

## 408 **DISCUSSION**

409           The main findings of our study can be summarized as follows: (i) we developed and  
410 internally validated EchoNet-RV, a DL model capable of accurately assessing RVFAC and  
411 identifying RV dysfunction from A4C echocardiographic videos, (ii) we externally validated  
412 EchoNet-RV's performance in two large datasets, confirming the model's generalizability across  
413 diverse patient populations, geographic regions, ultrasound machine vendors, and image  
414 qualities, (iii) we demonstrated that EchoNet-RV's prediction errors are lower than the inter-  
415 observer variability observed among human experts, (iv) we showed that, as a single-task model,  
416 EchoNet-RV can outperform multi-task models in estimating RVFAC and identifying RV  
417 dysfunction, and (v) we found that the predicted RVFAC values are significantly and  
418 independently associated with adverse clinical outcomes. Additionally, we released the code and  
419 model weights of EchoNet-RV to promote further research and facilitate deployment in other  
420 research or clinical environments.

421           AI has the potential to substantially enhance cardiac imaging workflows, particularly the  
422 challenging echocardiographic evaluation of RV function (7,27). Variability in acquisition  
423 protocols and technical settings, image analysis, and interpretation of RV parameters remains a  
424 major obstacle to the consistent clinical assessment of RV function across institutions and  
425 geographic regions (3). Standardized measurements are essential not only for accurate diagnosis  
426 and disease monitoring but also for guiding therapeutic decisions and ensuring reliable  
427 longitudinal follow-up. In this context, AI could be a valuable complement even to conventional  
428 core laboratory workflows by providing reproducible, objective, and scalable solutions for  
429 automating measurements and echocardiogram interpretation (28). While current commercially  
430 available AI tools for echocardiography support automated analysis of a limited set of RV

431 parameters, more advanced metrics and broader implementation and validation across diverse  
432 clinical environments remain necessary to fully realize the benefits of AI-driven RV function  
433 assessment (17,29). To date, no publicly available tool has been proposed that enables vendor-  
434 independent and consistent evaluation of RVFAC.

435         Despite their ease of use and reproducibility, the most recent American Society of  
436 Echocardiography guidelines emphasize the importance of not relying solely on measures of RV  
437 longitudinal shortening, such as TAPSE and S' (9). In specific clinical scenarios, such as  
438 following open-heart surgery or in patients with left ventricular systolic dysfunction, the  
439 mechanical pattern of RV contractions can shift toward a more radial orientation, and parameters  
440 quantifying solely the longitudinal function may underestimate global RV function (30,31).  
441 Conversely, in conditions characterized by RV pressure overload, longitudinal function often  
442 remains preserved in the initial phase of the disease, while radial contraction is the first to  
443 deteriorate (32). Although RVFAC is the most comprehensive two-dimensional parameter for  
444 assessing RV function, as it captures both longitudinal and radial shortening, as well as the  
445 contribution of the interventricular septum, it remains only the third most commonly adopted  
446 quantitative method for RV assessment, primarily due to its relatively limited reproducibility and  
447 the time-consuming nature of its measurement in routine clinical practice (3,4). Consistent with  
448 previous studies, we observed substantial inter-observer variability in RVFAC measurements,  
449 even among experienced readers. Notably, the prediction errors of EchoNet-RV compared to  
450 human measurements were lower than the inter-observer variability among human readers.  
451 While the model demonstrated acceptable discriminative power in differentiating normal RV  
452 function from RV dysfunction using a 35% RVFAC threshold, it is important to highlight that  
453 EchoNet-RV performs regression and estimates RVFAC on a continuous scale. This approach

454 allows for more granular assessment of RV function and may facilitate classification across the  
455 spectrum of dysfunction severity, aligning with recent guideline recommendations (9).  
456 Furthermore, the predicted RVFAC values were independently associated with both all-cause  
457 death and a composite endpoint of heart failure hospitalization or all-cause death, even after  
458 adjustment for relevant clinical covariates, including age, sex, coronary artery disease, heart  
459 failure, diabetes, chronic kidney disease, and left ventricular ejection fraction.

460 Intra-observer variability is the Achilles' heel of training AI models. When there is  
461 significant practice variation in holistic assessment, models trained in one center tend to  
462 generalize poorly to others. Moreover, when two clinicians disagree in their interpretation of the  
463 same image, the choice of ground-truth label can significantly affect model training (33).  
464 Additionally, the choice of threshold used for dichotomization also has a substantial impact on  
465 the performance metrics. Within this context, EchoNet-RV was compared to two large multi-task  
466 models trained on data from different institutions, both of which provide holistic assessments  
467 rather than direct quantitative measurements (20,21). Our results suggest that automated,  
468 measurement-driven evaluations continue to hold value, even when large AI models can provide  
469 holistic assessments (19). Just as a human cardiologist relies on both quantitative measurements  
470 and overall gestalt to arrive at a final clinical decision, AI models that combine measurement-  
471 driven and holistic evaluations will be essential for precise assessment of RV function.

472 EchoNet-RV was designed to mitigate errors arising from beat-to-beat variation by  
473 sampling multiple clips from each input video and averaging the individual predictions generated  
474 by its spatiotemporal CNN module from these clips to produce the final video-level output. For  
475 this test-time augmentation, we evaluated two sampling strategies: one similar to EchoNet-  
476 Dynamic's (13), in which the results of the semantic segmentation guided the sampling of clips,

477 and another, in which 5 clips were sampled randomly from each video. Interestingly, despite its  
478 simplicity and computational efficiency, the latter approach achieved marginally superior  
479 performance and was therefore adopted in the final EchoNet-RV model. Random sampling  
480 ensures that the number of analyzed clips is independent of the number of complete cardiac  
481 cycles, provides stable performance even when segmentation is unreliable (e.g., due to poor  
482 visibility of the RV free wall), and avoids the propagation of segmentation errors into the  
483 downstream task of RVFAC prediction. In addition, it eliminates the need for the segmentation  
484 step, thereby reducing processing time and computational demands. Nevertheless, although the  
485 semantic segmentation module is not used for RVFAC estimation, we retained it as a key  
486 component of EchoNet-RV, as its outputs may be valuable in other applications.

487         Although several segmentation-free DL models have recently been proposed for  
488 predicting RV morphological and functional parameters from echocardiographic videos  
489 (20,27,34), EchoNet-RV uniquely enables automated assessment of RVFAC – a key parameter  
490 of RV function – and demonstrated consistent performance across a wide range of image  
491 qualities, ultrasound machine vendors, and A4C definitions, including both standard and RV-  
492 focused views. This robustness underscores the model’s strong generalizability and highlights its  
493 potential for seamless integration into diverse real-world clinical environments, regardless of  
494 local imaging protocols or equipment.

495         EchoNet-RV also presents an unparalleled opportunity to enhance the objectivity of RV  
496 function assessment, particularly in clinical scenarios where operator bias may inadvertently  
497 influence interpretation. In contexts such as long-term disease monitoring or following surgical  
498 and transcatheter interventions, clinicians, motivated by the hope for positive outcomes, may  
499 unconsciously overestimate functional improvement, especially when faced with ambiguous or

500 technically challenging echocardiographic images. The visual presence of implanted devices or  
501 anatomical alterations can also hamper unbiased human evaluation. In contrast, EchoNet-RV  
502 offers a consistent, data-driven alternative that is unaffected by clinical expectations. Its ability to  
503 provide automated RVFAC measurements ensures standardized RV functional assessment across  
504 time points and institutions, enabling more accurate tracking of disease progression and response  
505 to therapy. As such, EchoNet-RV can serve as a critical adjunct in both routine clinical care and  
506 research. It holds particular promise for integration into point-of-care settings and screening  
507 programs, for example, in pulmonary hypertension, and can support an unbiased staging of  
508 overall cardiac dysfunction. This, in turn, may improve patient selection for advanced therapies  
509 such as left ventricular assist device implantation or transcatheter mitral and tricuspid valve  
510 interventions.

511

## 512 **Limitations**

513 Despite the promising results and strengths of our study, several limitations should be  
514 acknowledged. First, the inherent uncertainty of human-measured RVFAC values used as the  
515 reference standard may have introduced bias, thereby negatively affecting the observed  
516 performance, as these measurements represent only an estimate of the true physiological value.  
517 Importantly, EchoNet-RV still exhibited robust performance when evaluated using both the  
518 original and extended versions of the Bland-Altman analysis that account for uncertainty in the  
519 reference values. Moreover, although RVFAC reflects both longitudinal and radial components  
520 of RV function, it is unable to capture the ventricle's anteroposterior motion. Thus, although  
521 RVFAC is a guideline-endorsed parameter of RV function with well-established clinical  
522 relevance, other metrics that provide a more comprehensive assessment of global RV function

523 and have lower uncertainty may be considered as potential prediction targets in future studies.  
524 Second, EchoNet-RV was trained on data originating from a single healthcare system; therefore,  
525 the training dataset primarily represents the patient population treated at Stanford Health Care.  
526 Nevertheless, EchoNet-RV also demonstrated robust performance in two geographically distinct  
527 external datasets, supporting its generalizability and cross-healthcare system reliability. Finally,  
528 outcome data were available only for the Semmelweis dataset. Therefore, future studies are  
529 warranted to validate the observed associations between EchoNet-RV-predicted RVFAC values  
530 and clinical outcomes in larger, multicenter cohorts.

531 **CONCLUSIONS**

532           EchoNet-RV enables rapid and fully automated segmentation of the RV and assessment  
533 of RVFAC from A4C echocardiographic videos, demonstrating robust performance and  
534 generalizability across diverse populations. By providing objective, reproducible, and scalable  
535 quantification of RV function, EchoNet-RV has strong potential to become a valuable tool for  
536 echocardiogram interpretation and longitudinal disease surveillance.

537

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- 634

635 **TABLES**636 **Table 1** Clinical characteristics of the internal and external test sets

	<b>Internal test set</b>	<b>Semmelweis</b>	<b>MMH</b>
<b>Patients, n</b>	808	872	1,077
<b>Studies, n</b>	1,288	982	1,077
<b>Videos, n</b>	1,320	3,107	1,077
<b>Age, years</b>	60 (49-71)	47 (23-67)	65 (56-76)
<b>Males</b>	404 (50.0)	539 (61.8)	545 (50.6)
<b>Body mass index, kg/m<sup>2</sup></b>	25.0 (22.0-30.0)	25.0 (22.3-28.1)	25.1 (22.8-27.3)
<b>Body surface area, m<sup>2</sup></b>	1.82 (1.63-2.01)	1.90 (1.74-2.08)	1.65 (1.52-1.77)
<b>Systolic blood pressure, mmHg</b>	116 (106-132)	130 (118-140)	137 (123-153)
<b>Diastolic blood pressure, mmHg</b>	68 (62-77)	76 (69-84)	78 (70-86)
<b>Heart rate, 1/min</b>	68 (60-101)	71 (64-81)	72 (63-82)
<b>Coronary artery disease</b>	54 (6.7)	93 (10.7)	243 (22.6)
<b>Heart failure</b>	173 (21.4)	121 (13.9)	305 (28.3)
<b>Hypertension</b>	234 (30.0)	339 (38.9)	740 (68.7)
<b>Diabetes</b>	106 (13.1)	119 (13.6)	290 (26.9)
<b>Chronic kidney disease</b>	126 (15.6)	147 (16.9)	332 (30.8)
<b>LVEDV, mL</b>	82.1 (64.0-110.1)	130.1 (103.8-167.3)	95.6 (78.6-112.8)
<b>LVEDVi, mL/m<sup>2</sup></b>	45.1 (35.5-57.3)	69.5 (57.6-86.8)	57.1 (47.6-67.7)
<b>LVESV, mL</b>	33.9 (23.9-48.3)	55.9 (42.3-80.1)	33.2 (27-42)
<b>LVESVi, mL/m<sup>2</sup></b>	18.6 (13.4-26.3)	30.1 (23.1-40.2)	20.0 (16.0-25.2)
<b>LVEF, %</b>	59.5 (52.3-64.1)	57.2 (51-61.2)	64.7 (58.9-69.7)
<b>RV end-diastolic area, cm<sup>2</sup></b>	22.7 (17.6-28.6)	23.3 (19.7-27.5)	18.1 (15.4-20.9)
<b>RV end-systolic area, cm<sup>2</sup></b>	15.6 (11.4-21.1)	15.5 (12.5-18.5)	10.6 (9.1-12.6)
<b>RVFAC, %</b>	30.3 (21.9-37.8)	33.6 (29.3-38.5)	39.9 (34.9-44.8)

637 Values are median (interquartile range) or n (%). In the internal test set and the MMH dataset,

638 LV volumes and ejection fraction were measured using 2D echocardiography, whereas in the

639 Semmelweis dataset, they were measured using 3D echocardiography. In the Semmelweis

640 dataset, demographics and risk factors are reported at the patient level; vitals and LV  
641 echocardiographic parameters at the study level; and RV areas and RVFAC at the video level.  
642 LV – left ventricular, LVEDV – left ventricular end-diastolic volume, LVEDVi – left ventricular  
643 end-diastolic volume indexed to body surface area, LVEF – left ventricular ejection fraction,  
644 LVESV – left ventricular end-systolic volume, LVESVi – left ventricular end-systolic volume  
645 indexed to body surface area, MMH – MacKay Memorial Hospital, RV – right ventricular,  
646 RVFAC – right ventricular fractional area change

647 **Table 2** Comparison of EchoNet-RV’s prediction error with the beat-to-beat variability of  
 648 human measurements in the external test sets

	<b>EchoNet-RV</b>	<b>Beat-to-beat</b>	<b>P-value</b>
<b>Mean absolute difference, pp</b>	5.874 (5.729-6.021)	3.511 (3.409-3.612)	<0.001
<b>Standard error of measurement, pp</b>	3.746 (3.657-3.835)	2.130 (2.066-2.196)	<0.001
<b>Minimal detectable change, pp</b>	10.384 (10.137-10.631)	5.904 (5.727-6.088)	<0.001
<b>Coefficient of variation, %</b>	14.956 (14.598-15.326)	10.132 (9.826-10.448)	<0.001

649 This analysis only included videos (n=3,943) with RVFAC measurements in 2 or more cardiac  
 650 cycles. For each metric, 95% confidence intervals were calculated from 10,000 stratified  
 651 bootstrap resamples. Mean absolute differences were compared using paired Student’s t-test or  
 652 Wilcoxon signed-rank test, whereas the significance of the difference in standard error of  
 653 measurement, minimal detectable change, and coefficient of variation was determined using  
 654 bootstrap p-values.

655 Abbreviations as in Table 1.

656 **Table 3** Comparison of EchoNet-RV’s prediction error with the inter-reader variability of human  
 657 measurements in the external test sets

	<b>EchoNet-RV</b>	<b>Inter-reader</b>	<b>P-value</b>
<b>Mean absolute difference, pp</b>	6.126 (5.735–6.563)	9.699 (9.031–10.458)	<0.001
<b>Standard error of measurement, pp</b>	3.063 (2.868–3.282)	4.849 (4.515–5.229)	<0.001
<b>Minimal detectable change, pp</b>	8.490 (7.948–9.096)	13.442 (12.516–14.495)	<0.001
<b>Coefficient of variation, %</b>	12.568 (11.713–13.573)	17.651 (16.475–19.015)	<0.001

658 This analysis included 250-250 randomly selected videos from the MMH and Semmelweis  
 659 datasets. In each of these 500 videos, RVFAC was remeasured by a second reader blinded to the  
 660 first reader’s measurements. For each metric, 95% confidence intervals were calculated from  
 661 10,000 stratified bootstrap resamples. Mean absolute differences were compared using paired  
 662 Student’s t-test or Wilcoxon signed-rank test, whereas the significance of the difference in  
 663 standard error of measurement, minimal detectable change, and coefficient of variation was  
 664 determined using bootstrap p-values.

665 Abbreviations as in Table 1.

666 **Table 4** Performance of EchoNet-RV, EchoPrime, and PanEcho in the external test sets

	<b>EchoNet-RV</b>	<b>EchoPrime</b>	<b>PanEcho</b>
<b>Semmelweis (video-level)</b>			
MAE, pp	5.830 (5.670–5.992)	6.171 (6.002–6.339)	-
ICC	0.481 (0.452–0.509)	0.423 (0.394–0.450)	-
AUC	0.727 (0.709–0.744)	0.683 (0.664–0.701)	0.673 (0.654–0.692)
<b>Semmelweis (study-level)</b>			
MAE, pp	4.744 (4.541–4.943)	5.475 (5.214–5.743)	-
ICC	0.573 (0.526–0.617)	0.488 (0.437–0.534)	-
AUC	0.770 (0.746–0.794)	0.714 (0.681–0.745)	0.687 (0.653–0.720)
<b>MMH</b>			
MAE, pp	6.362 (6.064–6.660)	6.728 (6.406–7.048)	-
ICC	0.301 (0.243–0.356)	0.192 (0.127–0.253)	-
AUC	0.684 (0.648–0.719)	0.652 (0.614–0.690)	0.657 (0.619–0.695)

667 Performance metrics are reported with their corresponding 95% confidence intervals computed  
 668 using 10,000 bootstrapped samples. AUCs are reported for identifying videos/studies with an  
 669 actual RVFAC of less than 35%.

670 AUC – area under the receiver operating characteristic curve, ICC – intra-class correlation  
 671 coefficient, MAE – mean absolute error, pp – percentage point; other abbreviations as in Table 1.

672 **Table 5** Associations between the EchoNet-RV-predicted RVFAC values and the composite of  
 673 heart failure hospitalization or all-cause death

	<b>Univariable Cox regression</b>		<b>Multivariable Cox regression</b>	
	HR (95% CI)	P-value	HR (95% CI)	P-value
Age	1.072 (1.059–1.085)	<0.001	1.060 (1.043–1.077)	<0.001
Male sex	1.528 (1.041–2.244)	0.030	1.059 (0.703–1.595)	0.783
Coronary artery disease	4.204 (3.197–5.528)	<0.001	1.257 (0.896–1.762)	0.185
Heart failure	6.980 (4.876–9.992)	<0.001	1.301 (0.725–2.336)	0.377
Hypertension	6.943(4.529–10.644)	<0.001	1.155 (0.701–1.904)	0.571
Diabetes	4.871 (3.385–7.009)	<0.001	1.598 (1.086–2.350)	0.017
Chronic kidney disease	1.669 (1.112–2.505)	0.013	0.741 (0.483–1.136)	0.169
LVEF	0.936 (0.926–0.946)	<0.001	0.990 (0.969–1.011)	0.342
EchoNet-RV-predicted RVFAC	0.877 (0.855–0.900)	<0.001	0.943 (0.912–0.975)	<0.001

674 CI – confidence interval, HR – hazard ratio; other abbreviations as in Table 1.

675 **Table 6** Associations between the EchoNet-RV-predicted RVFAC values and all-cause death

	<b>Univariable Cox regression</b>		<b>Multivariable Cox regression</b>	
	HR (95% CI)	P-value	HR (95% CI)	P-value
Age	1.074 (1.059–1.088)	<0.001	1.061 (1.043–1.079)	<0.001
Male sex	1.567 (1.039–2.365)	0.032	1.076 (0.695–1.666)	0.742
Coronary artery disease	4.256 (3.208–5.647)	<0.001	1.364 (0.964–1.932)	0.080
Heart failure	6.744 (4.609–9.868)	<0.001	1.508 (0.790–2.879)	0.213
Hypertension	7.319 (4.616–11.606)	<0.001	1.237 (0.725–2.111)	0.434
Diabetes	4.931 (3.348–7.263)	<0.001	1.546 (1.029–2.325)	0.036
Chronic kidney disease	1.923 (1.264–2.926)	0.002	0.912 (0.586–1.419)	0.683
LVEF	0.940 (0.929–0.951)	<0.001	1.003 (0.980–1.026)	0.801
EchoNet-RV-predicted RVFAC	0.877 (0.854–0.901)	<0.001	0.932 (0.899–0.965)	<0.001

676 CI – confidence interval, HR – hazard ratio; other abbreviations as in Table 1.

677 **FIGURES**

678

679 **Central Illustration** AI-enabled echocardiographic assessment of RV function

680 In this study, we developed a novel deep learning model – EchoNet-RV – to segment the RV in  
681 A4C echocardiographic videos and estimate RVFAC. The model was trained and internally  
682 tested in 8,489 A4C echocardiographic videos from a single healthcare system. Its performance  
683 was evaluated on two international external test sets of 3,107 and 1,077 A4C videos from two  
684 separate centers. Additionally, the associations between the predicted RVFAC values and the  
685 composite endpoint of HF hospitalization or all-cause death were also analyzed in the first  
686 external test set.

687 A4C – apical 4-chamber view, HF – heart failure, MMH – MacKay Memorial Hospital, RV –  
688 right ventricle, RVFAC – right ventricular fractional area change

689

690 **Figure 1** Methods and results of segmentation

691 (A) Weakly supervised training of the semantic segmentation module using human expert  
692 tracings of RV areas on ED and ES frames and both annotated and non-annotated frames of the  
693 input video. (B) Segmented RV areas for all frames of a video from a patient in sinus rhythm and  
694 another from a patient in atrial fibrillation. (C) Performance of EchoNet-RV in segmenting the  
695 RV in the three test sets.

696 ED – end-diastolic, ES – end-systolic, MMH – MacKay Memorial Hospital, RV – right  
697 ventricular

698

699 **Figure 2** Schematic illustration of the two test-time augmentation strategies tested in the study  
700 (A) In the first approach, each ventricular contraction was identified by selecting the frames  
701 between the largest and smallest RV areas predicted by the semantic segmentation module. For  
702 each identified contraction (i.e., beat), 32-frame video clips centred around the ventricular  
703 contraction were obtained and processed by the spatiotemporal CNN module to produce **beat-to-**  
704 **beat** estimates of RVFAC, which were then averaged to yield the final video-level output of  
705 EchoNet-RV. (B) The second approach did not rely on the segmentation model's outputs.  
706 Instead, 5 (possibly overlapping) 32-frame video clips were **randomly sampled** from each  
707 video, and individual predictions generated by the spatiotemporal CNN module from these 5  
708 clips were averaged to produce the final video-level model output.  
709 CNN – convolutional neural network, RVFAC – right ventricular fractional area change; other  
710 abbreviations as in Figure 1.

711

712 **Figure 3** Performance of EchoNet-RV in predicting RVFAC

713 (A) Scatter plots showing the predicted vs. human-measured RVFAC values. (B) Conventional  
714 Bland-Altman plots showing the agreement between the predicted and human-measured RVFAC  
715 values. (C) Results of the extended Bland-Altman analysis that incorporates inverse weighting,  
716 defining a clinically relevant range of interest (RVFAC of 15–45%), and quantifying the trend  
717 between means and differences.

718 ICC – intraclass correlation coefficient, LOA – limit of agreement, MAE – mean absolute error,  
719 pp – percentage points; other abbreviations as in Figures 1 and 2.

720

721 **Figure 4** Performance of EchoNet-RV in predicting RVFAC in different subgroups of the  
722 external test sets

723 A4C – apical 4-chamber view; other abbreviations as in Figures 1 and 3.

724

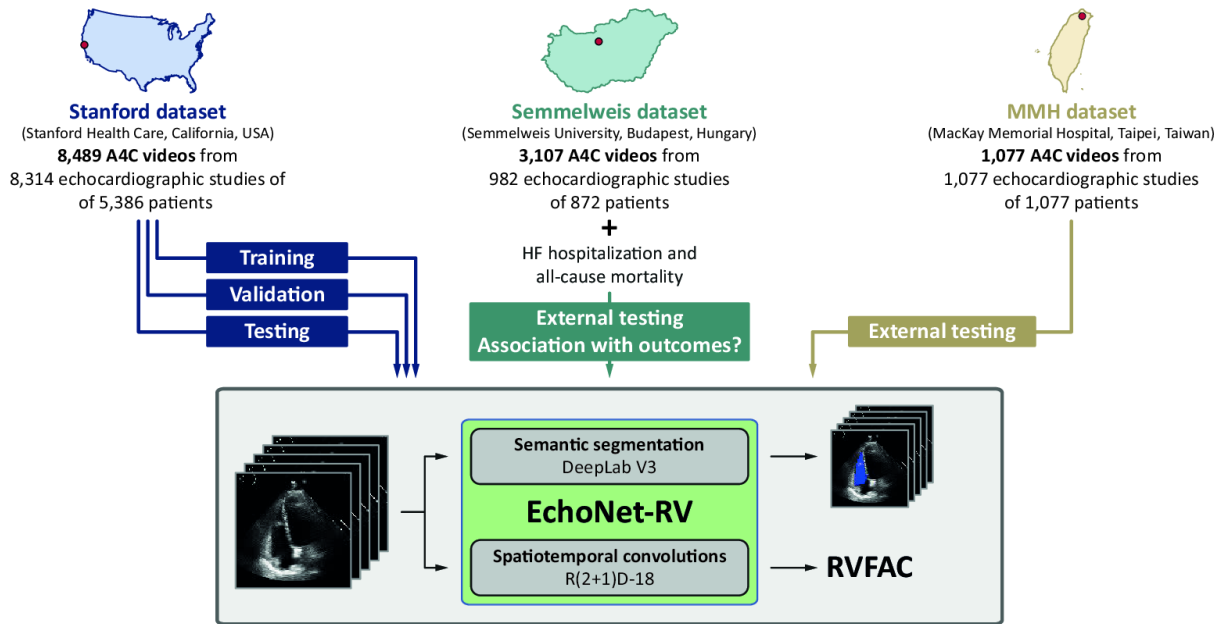
725 **Figure 5** Receiver operating characteristic curves illustrating the performance of EchoNet-RV in  
726 identifying RV dysfunction

727 AUC – area under the receiver operating characteristic curve; other abbreviations as in Figure 1.

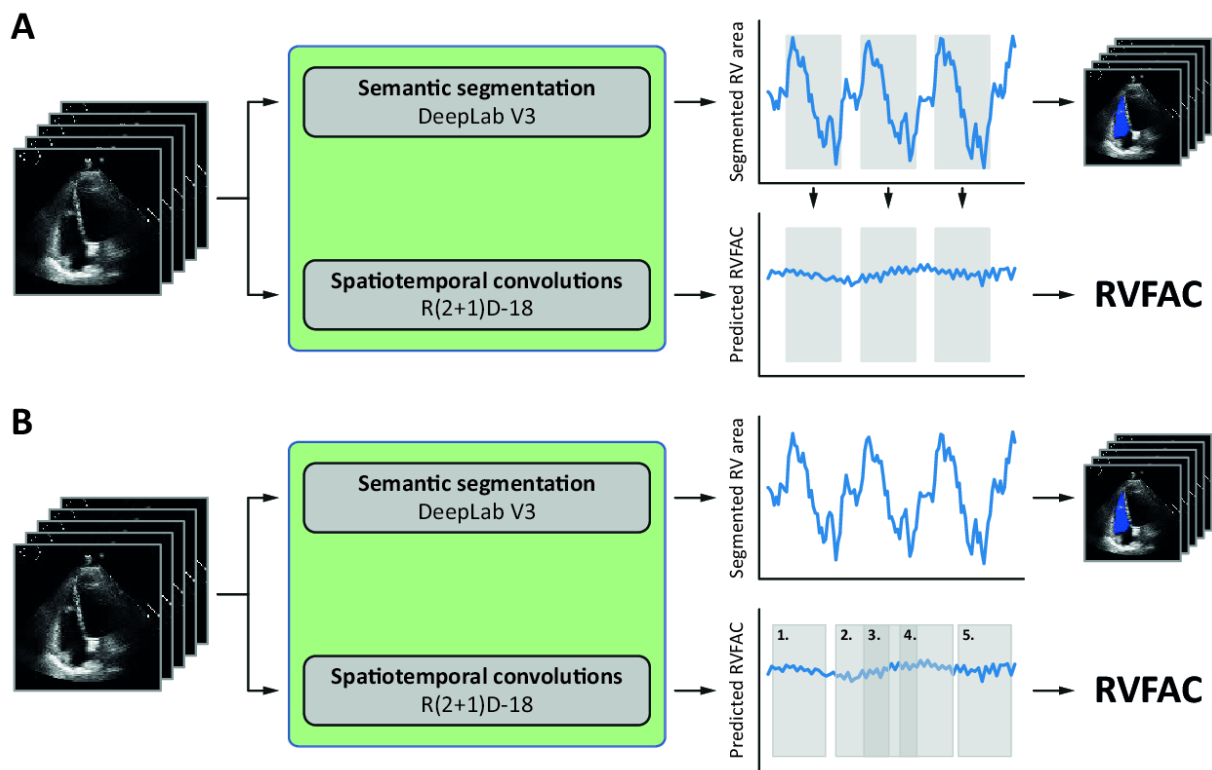
728

729 **Figure 6** Kaplan-Meier curves showing the event-free survival of patient subgroups in the  
730 Semmelweis dataset

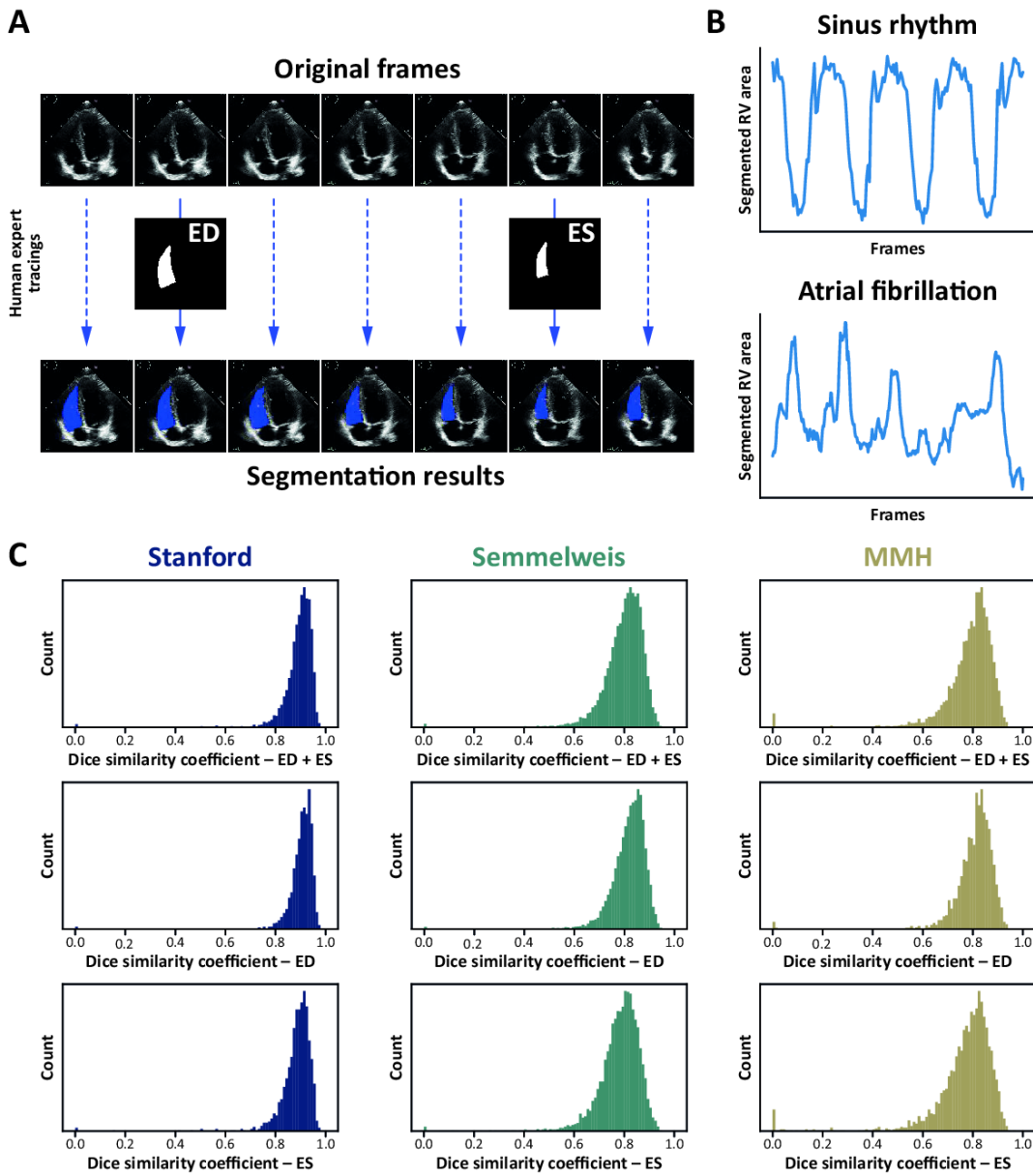
731 Abbreviations as in Figure 2.



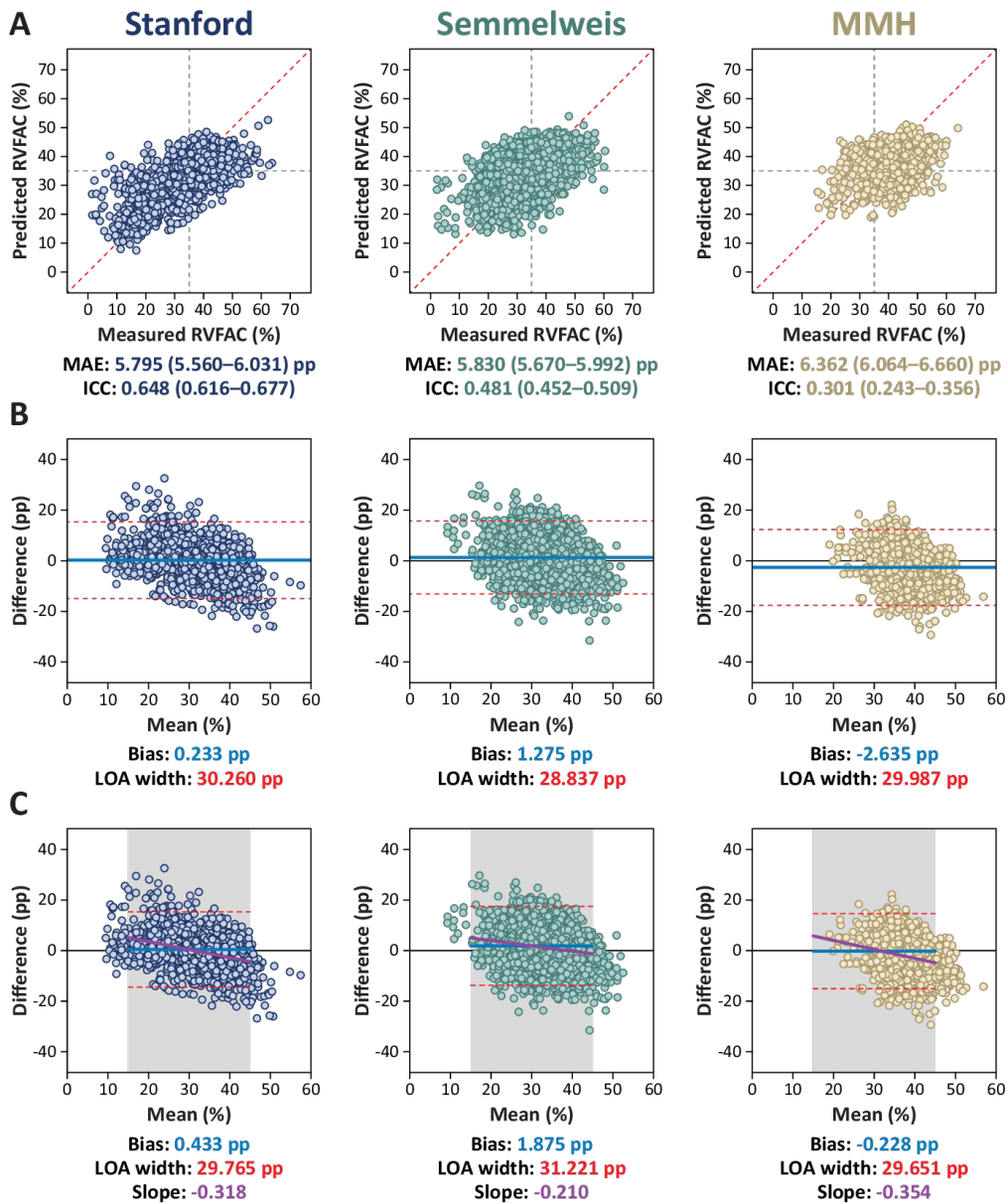
**Central Illustration:** AI-enabled echocardiographic assessment of RV function



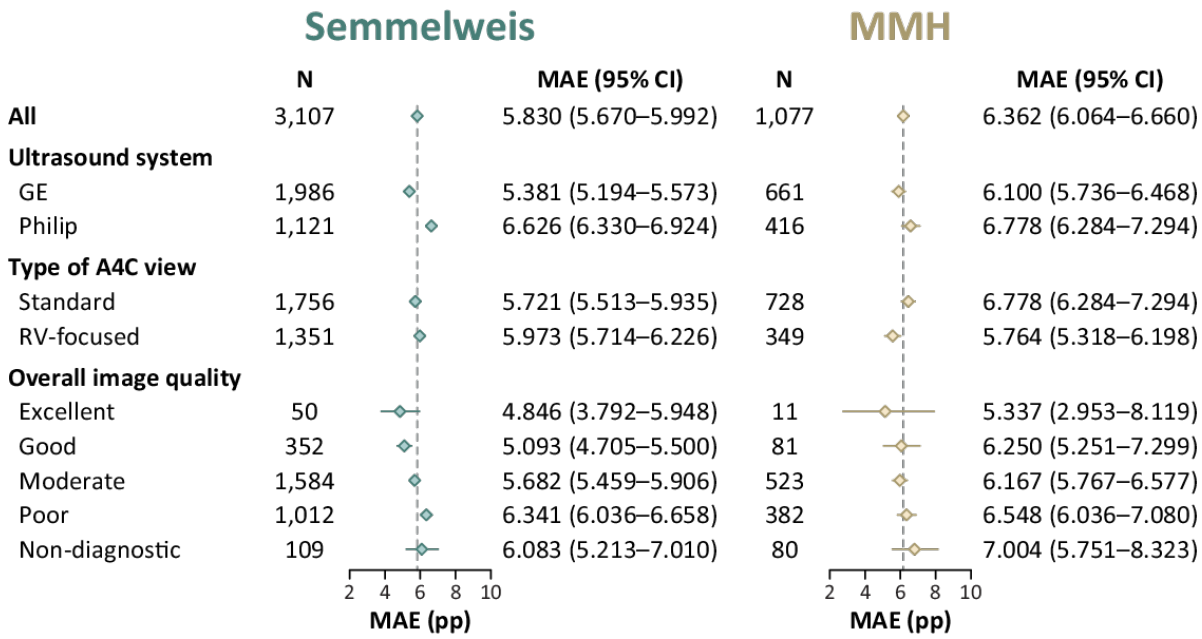
**Figure 1:** Methods and results of segmentation



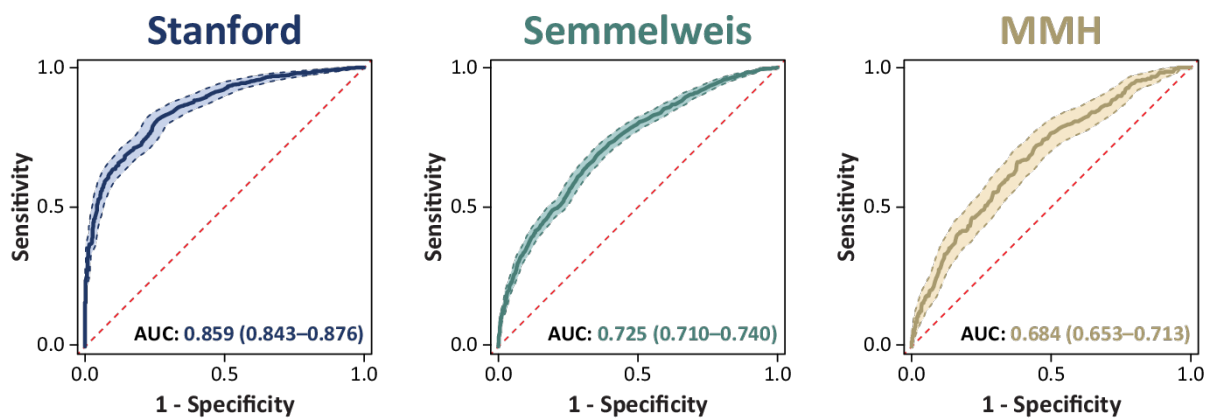
**Figure 2:** Schematic illustration of the two test-time augmentation strategies tested in the study



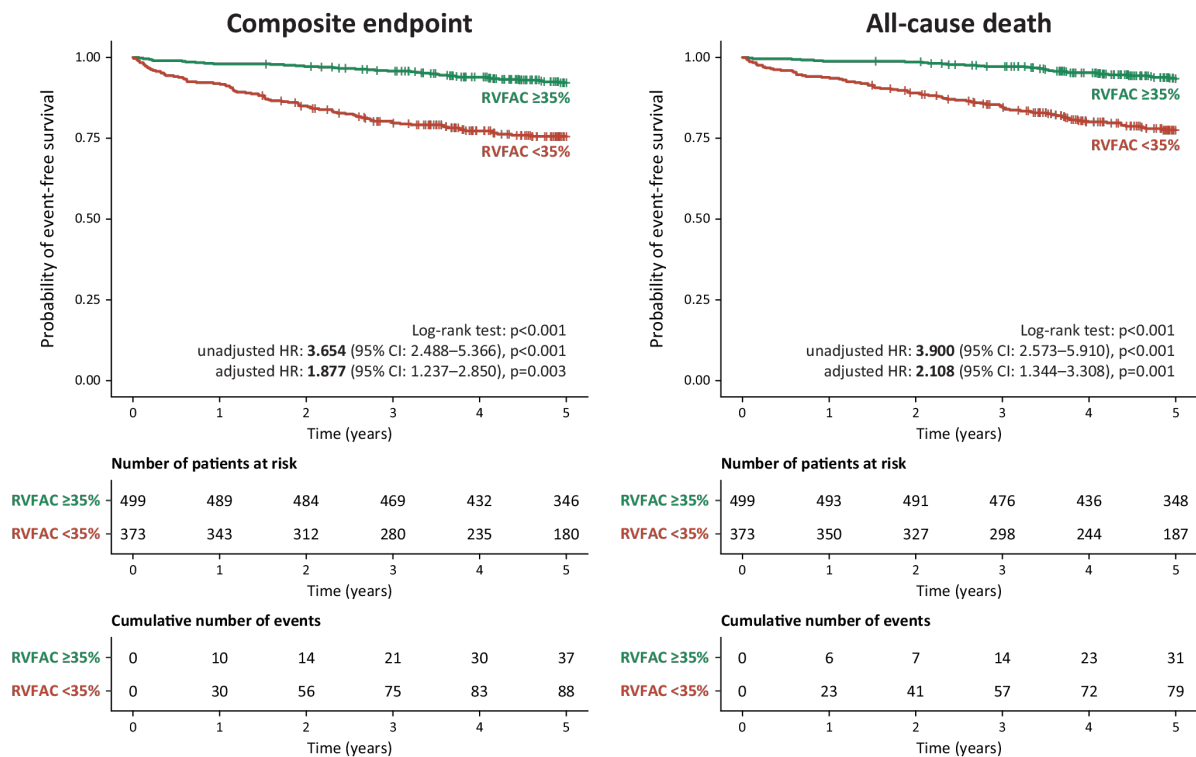
**Figure 3:** Performance of EchoNet-RV in predicting RVFAC



**Figure 4:** Performance of EchoNet-RV in predicting RVFAC in different subgroups of the external test sets



**Figure 5:** Receiver operating characteristic curves illustrating the performance of EchoNet-RV in identifying RV dysfunction



**Figure 6:** Kaplan-Meier curves showing the event-free survival of patient subgroups in the Semmelweis dataset